

1 **Cortical and trabecular bone analysis of professional dancers using**
2 **3D-DXA: a case–control Study**

3 **Running title: Cortical and trabecular bone analysis of professional dancers**

4 **Keywords: Bone density, DXA, dance training, osteoporosis, athletes**

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32 **Cortical and trabecular bone analysis of professional dancers using 3D-**
33 **DXA: a case-control Study**

34 Abstract

35 Introduction: Given the lack of relevant data, the aim of this study was to
36 examine femur cortical and trabecular bone in female and male professional
37 ballet dancers.

38 Material and methods: 40 professional ballet dancers and 40 sex- and age-
39 matched non-exercising controls volunteered. Femoral bone density was
40 scanned by dual-energy X-ray absorptiometry (DXA) scan. A 3D-DXA
41 software was used to analyse trabecular and cortical bone. Anthropometry,
42 maturation (Tanner staging), menstrual parameters (age at menarche and
43 primary amenorrhea), energy availability and nutritional analysis (3-day
44 record) were also assessed.

45 Results: Compared to non-exercising participants, dancers exhibited
46 significantly higher volumetric density for integral, cortical and trabecular
47 bone, and thicker cortex at the femur. Ballet dancers demonstrated lower body
48 weight compared to controls ($p < 0.01$). Female dancers had their menarche later
49 than controls, and the prevalence of primary amenorrhea were significantly
50 higher in dancers than controls ($p < 0.01$). Dancer's energy availability was
51 below the normal range (< 30 kcal/kgFFM/day).

52 Conclusions: Despite the presence of certain osteoporosis risk factors such as
53 low energy availability, primary amenorrhoea and lower body weight,
54 professional ballet dancers revealed higher bone density for both cortical and
55 trabecular bone compartments compared to controls.

56 Keywords: Bone density, DXA, dance training, osteoporosis, athletes

57

58 **Introduction**

59 Osteoporosis is characterized by deterioration of bone structure, leading to increased
60 risk of fracture due to bone mass loss (U.S. Department of Health and Human
61 Services, 2004). This condition is more frequent in the elderly and postmenopausal
62 women (NIH Consensus Development Panel on Osteoporosis Prevention, 2001).
63 Several studies have been reporting that exercise (particularly during the growing
64 years) increases bone mineral density (BMD) and prevents osteoporosis in later life
65 (Burrows, 2007; Cadore, Brentano, & Krueel, 2005). Weight-bearing exercise seems
66 to be the most effective physical activity for bone formation enhancement (Matthews
67 et al., 2006; Shanb and Youssef, 2014). However, it appears that exercise affects
68 differently the skeleton depending on the region of the bone; it has been suggested
69 that the effects of weight bearing exercise are more pronounced at cortical than at the
70 trabecular area of the lumbar spine (Mora et al., 1994). However, other studies
71 involving athletes have suggested that exercise affects equally cortical and trabecular
72 areas (Ireland et al., 2013; Wilks et al., 2009). Dancing, for instance, is characterised
73 by high levels of muscular strength, jumps, rapid turns, and high levels of physical
74 fitness (Allen, Nevill, Brooks, Koutedakis, & Wyon, 2013; Angioi, Metsios,
75 Koutedakis, & Wyon, 2009; Angioi, Metsios, Twitchett, Koutedakis, & Wyon, 2009;
76 Koutedakis, Frischknecht, Vrbova, Sharp, & Budgett, 1995; Koutedakis and
77 Jamurtas, 2004; Koutedakis et al., 1999; E. Twitchett et al., 2010; E. A. Twitchett,
78 Koutedakis, & Wyon, 2009); these types of movements are known to induce a
79 thicker cortical bone compartment (Nikander et al., 2009). Nevertheless, dancing is
80 also considered an aesthetic activity where low body weight and body characteristics
81 are essential for performance. Literature on the topic suggests that elite dancers may
82 restrict their diet (decreasing energy and/or nutrient intake), which may lead to low

83 body weight and/or negative energy balance (Koutedakis and Jamurtas, 2004). This
84 low energy intake can negatively affect bone, particularly the trabecular bone (Ikeda
85 et al., 2016). Indeed, it has been suggested that trabecular bone is a metabolic
86 compartment, depending mainly on hormonal or metabolic factors (Mora, et al.,
87 1994). Therefore, it seems that dancing has inherent characteristics that may enhance
88 bone formation at cortical areas, but may also negatively affect the trabecular
89 compartment. Studies on dancers' bone health have been showing conflicting results,
90 i.e. some studies suggest that professional dancers have lower BMD compared to
91 controls or normative values, whereas others suggest that professional dancers have
92 higher BMD (Amorim et al., 2015). No studies have been identified thus far
93 reporting cortical and/or trabecular bone mass in elite dancers. However, it has been
94 reported that eumenorrheic non-elite dancers have higher distal tibial trabecular
95 BMD their oligo/amenorrheic counterparts (To, Wong, & Lam, 2005). Studies on
96 other athletic populations show that amenorrheic athletes had lower trabecular
97 volumetric bone mineral density (vBMD) at distal radius compared to non-athletes
98 (similar cortical vBMD was found at the same anatomical site), whereas similar
99 values of both trabecular and cortical vBMD were found at the distal tibia
100 (Ackerman et al., 2012).

101 Dual Energy X-ray Absorptiometry (DXA) is the most commonly used
102 clinical method of BMD assessment. DXA, however, does not measure the
103 volumetric BMD, but quantifies a 2D areal BMD in a projective image of the bone
104 content. As a result, cortical and trabecular bone cannot be separately assessed.
105 Advanced analytic methods have been proposed for obtaining additional information
106 from standard DXA scans, which, nevertheless, have their own limitations. For
107 example, Hip Structural Analysis (HSA) (Beck, Ruff, Warden, Scott, & Rao, 1990)

108 uses assumptions about the bone geometry and BMD distribution to compute cross-
109 sectional parameters related to bone strength. Trabecular Bone Score (TBS)
110 (Pothuaud, Carceller, & Hans, 2008) is a textural parameter correlated with bone
111 microarchitecture that can be measured in spine DXA scans. Recently, 3D modelling
112 techniques have been proposed to assess the trabecular and cortical bone from hip
113 DXA scans (Humbert et al., 2017; Väänänen, Grassi, Flivik, Jurvelin, & Isaksson,
114 2015). These “3D-DXA” methods use statistical appearance models together with
115 registration algorithms to model the femur shape and density in 3D and assess both
116 the cortical and trabecular bone from standard hip DXA scans.

117 The aim of this study is to assess cortical and trabecular bone at the femur in
118 female and male professional ballet dancers using 3D-DXA.

119 **Methods**

120 *Participants*

121 All professional dancers performing in a professional ballet company (full-time
122 dancing; 6-8 hours of training per day, 5 days per week; these dancers started their
123 full-time training at the age of 10) were invited to participate; the total of 42
124 individuals (68.3%) volunteered. They completed a questionnaire concerning their
125 ethnicity, medical history, and past/current calcium/vitamin D supplementation.
126 Eligible criteria included dancers of white European origin, with no illnesses or
127 treatments that might affect bone metabolism, not taking medication known to affect
128 bone metabolism and no calcium/vitamin D supplementation (one professional
129 dancer was excluded). Women taking oral contraceptives and hormonal therapy were
130 also excluded (one professional dancer). Based on these criteria, the studied
131 population consisted of 40 professional ballet dancers (30 female and 10 male).

132 Non-exercising participants were also recruited from a local University to act
133 as controls. Eligibility criteria for controls were set according to dancers'
134 characteristics, i.e. same sex, age (defined as decimal age; 12-months difference of a
135 dancer) and race (white European-Caucasian). Exclusion criteria included
136 participation in organised physical activities/sports (i.e. participants were excluded if
137 they were involved in any form of organised exercise). Control participation was also
138 restricted to those who had received/were receiving medications known to affect
139 bone metabolism and/or reported illnesses/treatments that might affect bone
140 metabolism. The total of 40 controls fulfilled the aforementioned criteria.

141 All participants provided signed informed consent according to the
142 Declaration of Helsinki. The study was approved by the ethics committee of the
143 Regional Administration of Health of Lisbon, Portugal (Proc.063/CES/INV/2012).

144

145 *Anthropometry, maturation assessment, menstrual, energy expenditure, and*
146 *nutritional analysis*

147 Chronological age (obtained as decimal age) and anthropometry measurements were
148 obtained. Height and body weight were measured in t-shirt, shorts and bare feet
149 using a stadiometer (Seca, Seca217 portable stadiometer, Hamburg, Germany) with
150 accuracy of 0.1 cm and an electric scale (TANITA BC-418 MA Segmental Body
151 Composition Analyser; Tanita Corporation, Tokyo, Japan) with an accuracy of 0.1
152 kg.

153 All female participants completed a questionnaire to determine age at
154 menarche, regularity of menstrual cycles and consumption of contraceptives.
155 Amenorrhea was defined as the absence of menses for three consecutive months,
156 whereas oligomenorrhea was considered when menstrual cycles occurred at intervals
157 of greater than 35 days.

158 Energy expenditure and energy intake were only assessed in professional
159 dancers. Professional dancers' energy expenditure was estimated using
160 accelerometer (SenseWear, Bodymedia SenseWear MF Armband Profi-Schrittzähler
161 Fitnesstracker, Germany), the validity and accuracy of which appear elsewhere
162 (Brazeau et al., 2014). Each dancer used the device for 7 consecutive days. The
163 accelerometer was used on the upper right arm for approximately 24-hours. During
164 the same period, nutrient intakes were recorded via a 3-day food diary. Participants
165 were instructed to record all food and beverages consumed during two week days
166 and one weekend day following appropriate instructions. The software Food
167 Processor SQL Edition, version 9.8.1 was used to estimate average energy and
168 calcium intakes. Energy availability was further estimated using standard protocols
169 (<http://www.femaleathletetriad.org/calculators/>); information on dietary energy
170 intake (provided by the food diary), exercise energy expenditure (information
171 retrieved from the accelerometer), and body fat percentage (measured by DXA) was
172 used to estimate energy availability.

173

174 ***Bone mass measurements***

175 BMD (g/cm^2) and bone mineral content (BMC) (g) were determined using DXA.
176 Hip DXA scans were administered to assess bone parameters at the proximal femur,
177 and total body DXA scans were used to estimate fat mass and lean mass. All DXA
178 scans were performed using a GE Lunar Prodigy (GE Medical Systems, Madison,
179 WI) and ENCORE software (version 12.3, Prodigy; Lunar Corp, Madison, WI). The
180 coefficients of variations measured in our centre was 1.0% for both total femur BMD
181 and total body. The same certified technician performed all DXA scans.

182

183 ***3D-DXA modelling***

184 3D-DXA software (version 2.2, Galgo Medical) was utilised to assess trabecular
185 macrostructure and cortex of all participants (both professional dancers and
186 controls). This software uses a statistical shape and density model of the proximal
187 femur built from a database of Quantitative Computed Tomography (QCT) images.
188 The algorithm registers the 3D statistical model onto the DXA scan to obtain a 3D
189 participant-specific model of the proximal femur shape and BMD distribution. The
190 cortical thickness and density was computed by fitting a function of the cortical
191 thickness and density, location of the cortex, density of surrounding tissues, and
192 imaging blur to the density profile computed along the normal vector at each node of
193 the proximal femur surface mesh (Humbert, Martelli, et al., 2017). Figure 1 shows
194 the main steps of the modelling process and the software interface. The vBMD,
195 BMC and volume can be computed at the total femur (union of the neck, trochanter
196 and shaft) region of interest for the trabecular, cortical and integral (trabecular and
197 cortical) bone. The mean cortical thickness was computed at the total femur region of
198 interest. The accuracy of models and measurements provided by the 3D-DXA
199 software algorithm was evaluated against QCT in previous work (Humbert, Martelli,
200 et al., 2017). Briefly, integral, trabecular, and cortical vBMD computed by QCT and
201 3D-DXA at total femur have shown correlation coefficients of 0.95, 0.86, and 0.93,
202 respectively. The correlation coefficient between cortical thickness computed by 3D-
203 DXA and QCT at total femur was 0.91. The method was evaluated in men and
204 women with normal bone density, osteopenia and osteoporosis (mean age of $57.5 \pm$
205 13.5 years [23 years–91 years]). The least significant changes (LSC) for the 3D-
206 DXA measurements (evaluated in postmenopausal women) were 16.8 mg/cm^3 for
207 the integral vBMD, 15.5 mg/cm^3 for the trabecular vBMD, 16.6 mg/cm^3 for the

208 cortical vBMD (total femur), and 0.057 mm for the cortical thickness (Humbert, Di
209 Gregorio, & Del Rio, 2017).

210

211 *Statistical analyses*

212 3D-DXA and DXA measurements were computed for all participants (professional
213 dancers and controls); unpaired two-sample t-test was used, after checking for
214 normality, to compare measurements between groups. In case significant differences
215 were found between participant characteristics (age, weight or height), the variables
216 were treated as potential confounding parameters. ANCOVA was used to compare
217 density measurements between groups after adjusting for confounding variables.
218 ANCOVA was used to analyse the differences after adjusting for confounding
219 variables. Average cortical thickness and density mapping were generated for both
220 groups. The statically significance of the differences found at each vertex of the
221 femoral shape was analysed using Student's t-test. To compare the volumetric
222 densities of both groups, the average 3D-DXA density instance was computed for
223 each group and registered onto the average femoral shape for the group. A frontal
224 slice was computed for each group for comparison purposes. The R 3.3.2 software
225 (www.r-project.org) was used for all statistical analyses, whilst the statistical
226 significance was set at $p < 0.05$.

227

228 **Results**

229 Descriptive general characteristics of all participants appear in Table 1. Professional
230 ballet dancers demonstrated similar age and height, but showed significantly lower
231 body weight ($p < 0.01$) and fat mass ($p < 0.001$) compared to controls. Also, dancers'
232 age at menarche and primary amenorrhea were significantly higher than controls

233 ($p<0.01$). Energy intake and energy availability in dancers were 1728.8 ± 607.9
234 Kcal/day and 26.9 ± 15.4 kcal/kgFFM/day, respectively.

235 3D-DXA and DXA measurements are shown in Table 2. Since a significant
236 difference was found between professional dancers and controls regarding body
237 weight, this variable was included as a potential confounding parameter. Professional
238 dancers revealed significantly higher vBMD than controls (8.1% higher; $p=0.036$,
239 without adjusting for body weight). Specifically, both cortical and trabecular vBMD
240 were significantly increased in dancers compared to controls (12.4% higher, $p=0.016$
241 and 2.3% higher, $p=0.037$, respectively). Compared to controls, professional dancers
242 had a thicker femoral cortex (5.4% thicker, $p=0.046$). After the adjustment for body
243 weight, all measured bone parameters (both DXA and 3D-DXA outcomes) showed
244 significant differences between dancers and controls ($p<0.05$; Table 2). The
245 anatomical distribution of the differences in cortical thickness and density between
246 dancers and controls is displayed in Figure 2. The mean frontal slice computed for
247 dancers and controls, as well as a difference image between both groups can be seen
248 in Figure 3.

249

250 **Discussion**

251 Existing literature has revealed rather conflicting results on professional dancers'
252 bone health, i.e. some studies highlight that dancers have low BMD, whereas others
253 show that dancers have greater BMD compared to controls. To our knowledge, this
254 is the first study investigating volumetric parameters at the femur (impact site) in a
255 sample of female and male professional ballet dancers. Using 3D-DXA, we found
256 evidence that, compared to non-exercising participants, professional ballet dancers
257 displayed higher vBMD for integral, cortical and trabecular bone, and thicker cortex

258 at the femur. This might indicate that professional dancing is capable of inducing
259 bone mass gains at both cortical and trabecular level, even in the presence of a
260 relatively low energy availability.

261 It is general believed that both female and male elite athletes are at risk for a
262 relative energy deficiency in sport (RED-S) (Mountjoy et al., 2014). Indeed, it has
263 been recently suggested that energy deficiency in relation to energy intake and
264 energy expenditure balance is a main factor that triggers several health concerns,
265 including low bone mass (Mountjoy, et al., 2014). The energy imbalance that elite
266 athletes may experience can affect negatively the hypothalamus, decreasing the
267 circulating levels of certain bone-related hormones, hindering further bone
268 mineralization (Locatelli and Bianchi, 2014). Accordingly, the training loads that
269 typically will enhance bone formation in elite athletes may be annulled due to the
270 presence of low energy availability and other well-known osteoporosis risk factors
271 such as low body weight and menstrual disturbances. The spectrum of low energy
272 availability, low body weight and, consequently, low BMD may mainly affect
273 participants involved in aesthetic sports whereas body characteristics are essential for
274 performance (Maimoun, Georgopoulos, & Sultan, 2014). Indeed, previous studies
275 demonstrated that athletes in aesthetic sports who experience amenorrhea (Robinson
276 et al., 1995) and have low energy availability may also have relatively low BMD
277 (Valentino et al., 2001). It has been showed that amenorrheic athletes have lower
278 BMD than eumenorrheic athletes (Ackerman, et al., 2012; Rencken, Chesnut, &
279 Drinkwater, 1996; Russell et al., 2009), and, consequently, impaired bone
280 microarchitecture (Ackerman et al., 2011; Micklesfield, Lambert, Fataar, Noakes, &
281 Myburgh, 1995; Tomten, Falch, Birkeland, Hemmersbach, & Hostmark, 1998). In
282 fact, energy availability of our professional ballet dancers was below the normal

283 range (i.e. <30 kcal/kgFFM/day), and their body weight was significantly lower
284 compared to controls. Further, the presence of primary amenorrhea, a well-known
285 osteoporosis risk factor, was significantly increased in female dancers compared to
286 matched controls. However, despite the presence of the aforementioned osteoporosis
287 risk factors, professional ballet dancers' bone mass was higher compared to sex- and
288 aged-matched controls. Unlike previous studies, this finding may indicate that dance
289 training stimuli is sufficient to counterbalance the potential negative effects of low
290 energy availability, low body weight and menstrual disturbances. Indeed, if these risk
291 factors were negatively affecting BMD in our professional ballet dancers, it would be
292 expected to find lower trabecular bone compared to controls as it has been reported
293 that this type of bone is a metabolic compartment, more sensitive to hormonal
294 imbalance (Mora, et al., 1994). Interestingly, the present study shows that
295 professional dancers revealed higher trabecular and cortical areas than controls. This
296 suggests that dance training might be able to induce bone anabolic adaptations at
297 both trabecular and cortical compartments. This is in line with available data on other
298 athletic populations showing that exercise is capable of inducing BMD gains in both
299 cortical and trabecular areas (Ireland, et al., 2013; Wilks, et al., 2009). It has also
300 been reported that femoral neck strength at the superolateral area is the most relevant
301 in fall-related fractures (Fuchs et al., 2017). Our professional dancers revealed higher
302 density in this area compared to controls, which might indicate reduced risk of
303 fractures.

304 It is difficult to compare the present findings with those from other studies as
305 the majority of the published reports have not examined volumetric bone mass
306 parameters in dancers (Burckhardt, Wynn, Krieg, Bagutti, & Faouzi, 2011; Hoch et
307 al., 2011; Khan et al., 1996; Matthews, et al., 2006; Robinson, et al., 1995); however,

308 recent studies showed that professional ballet dancers (both female and male) have
309 higher BMD at the femur compared to matched controls (Amorim, Koutedakis, et al.,
310 2017; Amorim, et al., 2015; To, et al., 2005). Using micro-finite element analysis
311 applied to high-resolution MRI, it was found that modern dance students (female)
312 have higher trabecular bone stiffness at the distal femur compared to controls,
313 suggesting a better adaptation to exercise stimuli of the trabecular bone compartment
314 rather than the cortical bone (Chang et al., 2013). However, this study examined
315 modern dance students. Due to differences in training regiments, selection criteria
316 and training loads, findings in modern and collegiate dance students might not be
317 transferable to professional ballet dancers. Indeed, unlike our dancers and collegiate
318 dancers, modern dance students did not revealed any osteoporosis risk factor (Chang,
319 et al., 2013).

320 The fact that our dancers demonstrated significantly higher cortical and
321 trabecular BMD at the femur does not exclude the possibility of a relatively low
322 BMD at other anatomical sites. It has been previously demonstrated that female
323 professional ballet dancers have lower BMD at the forearm (non-impact site)
324 compared to general population (Amorim, Koutedakis, et al., 2017). The same
325 phenotype has also been reported in relation to vocational dance students at the
326 forearm and lumbar spine (impact spine) (Amorim, Koutedakis, et al., 2017;
327 Amorim, Metsios, et al., 2017). The longitudinally assessment of cortical and
328 trabecular BMD at the aforementioned anatomical sites (particularly at the lumbar
329 spine as it is mainly constituted by trabecular bone) would provide insights on how
330 bone mass changes as dancers receive dance training stimuli. Furthermore, it would
331 also be of interest to report prevalence estimates of low energy availability and low

332 body weight, given that the report as mean \pm SD does not allow discrimination of the
333 true number of cases with osteoporosis risk factors.

334 The present study showed differences in cortical thickness and density
335 between the view anterior and posterior femur in both dancers and controls. One
336 potential explanation for these observations might be the fact that quadriceps
337 muscles are more often recruited during daily activities than hamstrings. This
338 frequent activation of the quadriceps might induce pressure forces at the anterior
339 femur unlike the posterior femur, increasing further bone formation at the anterior
340 face. In fact, research has shown that quadriceps muscles are stronger than
341 hamstrings for both non-athlete and athletic populations (Jung, Lee, Seo, & Song,
342 2017; Smidt, 1973; Sundby and Gorelick, 2014; Zvijac, Toriscelli, Merrick, Papp, &
343 Kiebzak, 2014).

344 The use of 3D-DXA could be insightful to monitor athletes, as it provides
345 information on the cortical and trabecular bone at an impact site. Nevertheless, the
346 present study has also some limitations regarding its methodology. 3D-DXA is a
347 modelling technique which is not as accurate as direct measurement techniques, such
348 as QCT or pQCT (at the tibia or radius). Further, the accuracy of 3D-DXA analyses
349 has not been specifically evaluated for elite dancers. Nevertheless, a previous study
350 showed that 3D-DXA provides accurate data for young healthy population (male and
351 female), compared to QCT (Humbert, Martelli, et al., 2017). Furthermore,
352 differences in integral BMC measured by 3D-DXA between professional dancers
353 and controls were higher than those found from DXA (12.6% and 5.1%,
354 respectively). The difference between BMC measurements obtained using the two
355 techniques might be related to the definition of the regions of interest. The 3D-DXA
356 total femur region was defined over the 3D subject-specific femoral shapes, while

357 the DXA total femur region was identified in the DXA scan. Another limitation of
358 the present study is its cross-sectional design, which means that causality cannot be
359 established. The use of a self-reported questionnaire to assess nutrition intake, as
360 well as the lack of data on energy intake and availability in controls, are further
361 limitations of the present study. The studied population mostly consisted of females
362 (n=29). The small number of male participants (n=11) did not allow us to conduct
363 meaningful statistics on this sub-cohort. However, preliminary analyses showed that
364 the male and female professional dancers of our cohort, when studied separately, had
365 higher areal bone mineral density, higher vBMD in the cortical, trabecular and
366 integral compartments, and thicker cortex, compared to controls, following the trends
367 observed for the entire cohort. Finally, we did not recorded fractures or injuries
368 among our dancers. However, in order to establish the clinical significance of our
369 findings, it would be of great interest for future studies to report the association
370 between low BMD and dance injuries.

371

372 **Conclusion**

373 Elite ballet dancing does not appear to have a deleterious effect on bone health.
374 Regardless of the presence of low energy availability and low body weight,
375 professional ballet dancers have higher BMD for both cortical and trabecular bone
376 compartments. This might indicate that professional dance training stimuli may
377 counterbalance the potential deleterious effects of the presence of osteoporosis risk
378 factors at the femur (impact site). Future studies should assess other impact (lumbar
379 spine) and non-impact (forearm) sites using longitudinal models.

380

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387

388 **Disclosure statement**

389 Ludovic Humbert is a stockholder at Galgo Medical.

390

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580

581 Table 1. General characteristics of the studied participants.

582 Table 2. Unadjusted and adjusted DXA and 3D-DXA parameters of total femur.

583 Figure 1. 3D-DXA modelling process and software interface. A) Registration of the
584 3D statistical model onto the hip DXA scan, attained by maximising the similarity
585 between the projection of the model and the DXA image. B) Measure density
586 variations along the normal vector at each node of the femur surface, and estimate
587 cortical thickness and density by fitting of a function of location of the cortex,
588 density of surrounding tissues, and imaging blur to the measure density variations. C)
589 Software interface showing the anatomical distribution of the cortical thickness.

590 Figure 2. Differences in cortical thickness (mm, top left, and percentage, top right)
591 and cortical density (mg/cm^3 , bottom left, and percentage, bottom right) between
592 professional dancers and controls. Colour-coded regions indicate statistically
593 significant differences. Regions with no significant differences are left in grey.

594 Figure 3. Front slice showing the average vBMD values in controls (left) and
595 professional dancers (middle), and average differences between both groups (right)
596 displayed only for the trabecular bone. The contour of the average shape in the
597 control group is shown in purple (right).